

Superhydrophobic paper-based microfluidic field-effect transistor biosensor functionalized with semiconducting single-walled carbon nanotube and DNAzyme for hypocalcemia diagnosis

Hui Wang¹, Ruipeng Chen¹, Fan Zhang^{1,2}, Zhixue Yu¹, Yue Wang¹, Zhonglin Tang¹, Liang Yang¹, Xiangfang Tang^{1*} and Benhai Xiong^{1*}

¹ State Key Laboratory of Animal Nutrition, Institute of Animal Science, Chinese Academy of Agricultural Sciences, Beijing 100193, China; wanghui10@caas.cn (H.W.); chen_ruipeng@yeah.net (R.C.); zhangfan19@139.com (F.Z.); 82101205310@caas.cn (Z.Y.); wangyue9313@163.com (Y.W.); tangzhonglin@caas.cn (Z.T.); yangliang@caas.cn (L.Y.)

² State Key Laboratory of Animal Nutrition, College of Animal Science and Technology, China Agricultural University, Beijing 100193, China

* Correspondence: tangxiangfang@caas.cn (X.T.); xionghbenhai@caas.cn (B.X.)

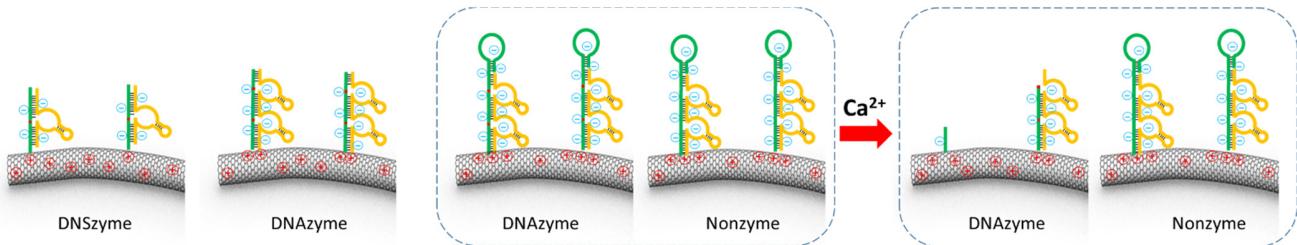


Figure S1. Mechanism of electrochemical field-effect biosensor for Ca^{2+} detection.

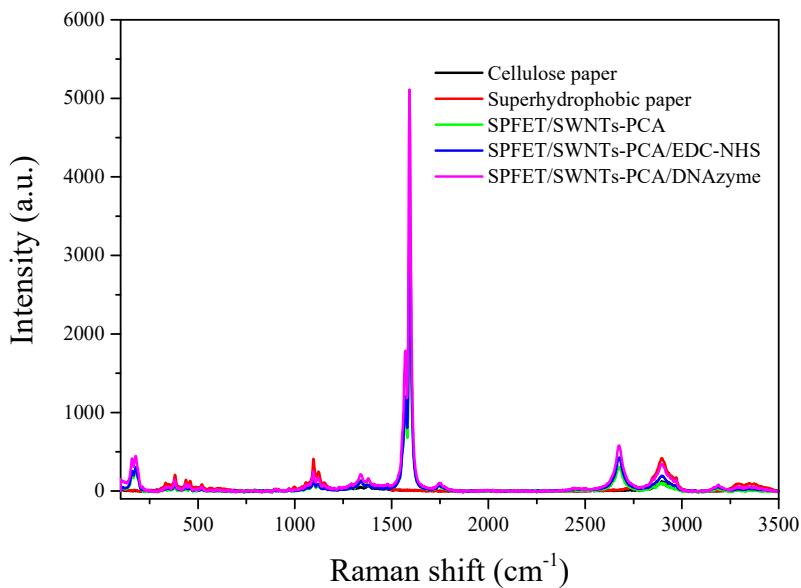


Figure S2. Raman spectra of cellulose paper before and after functionalized different materials: (a)Cellulose paper; (b)Superhydrophobic paper; (c)SPFET/SWNTs-PCA; (d)SPFET/SWNT-PCA/EDC-NHS and (e) SPFET/SWNT-PCA/DNAzyme.

Table S1. The ratios of different bands to G-band

	SWNT-PCA	EDC-NHS	DNAzyme
I_{RBM}/I_G	0.0984	0.0805	0.0814
I_D/I_G	0.0325	0.0286	0.0263
I_G/I_G	0.109621	0.114043	0.105141

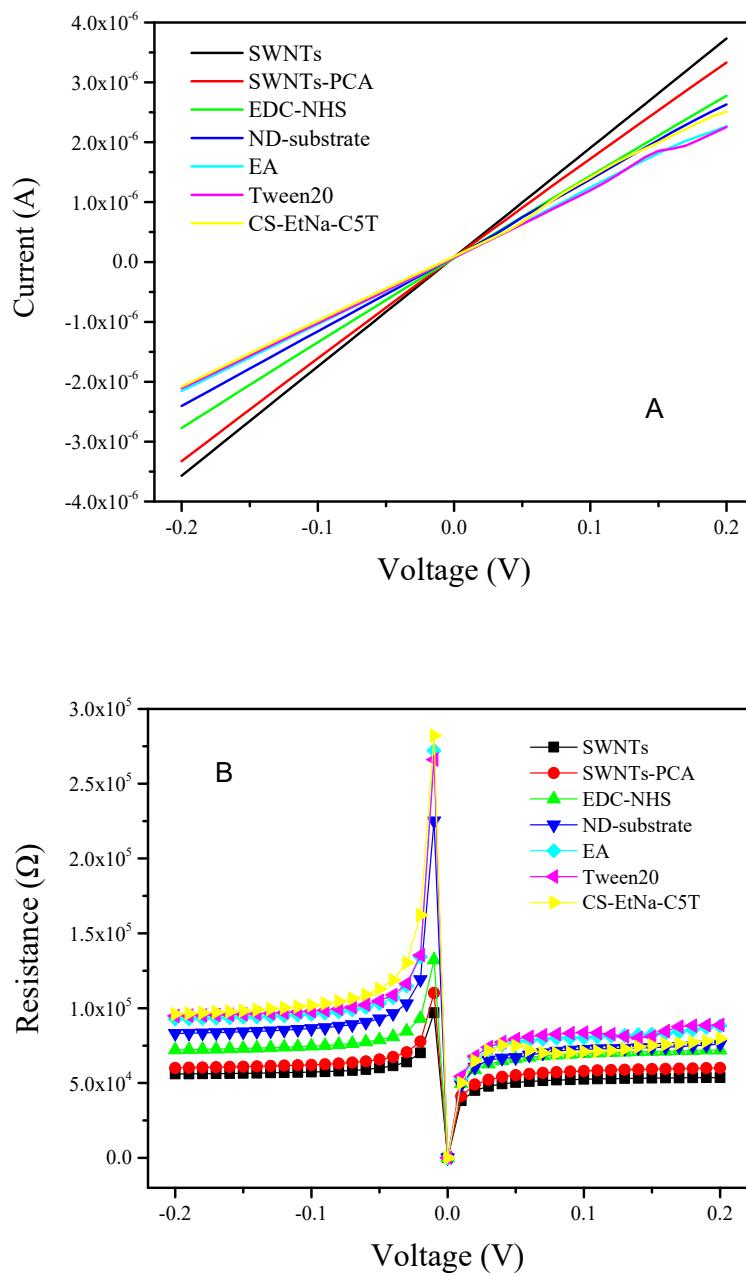


Figure S3. (A) $I_{DS}-V_{DS}$ and (B) Resistances of HPFET modified with different materials (SWNTs, PCA, EDC-NHS, ND-substrate, EA, Tween 20 and CS-EtNa-C5T) at different voltages.

Optimization

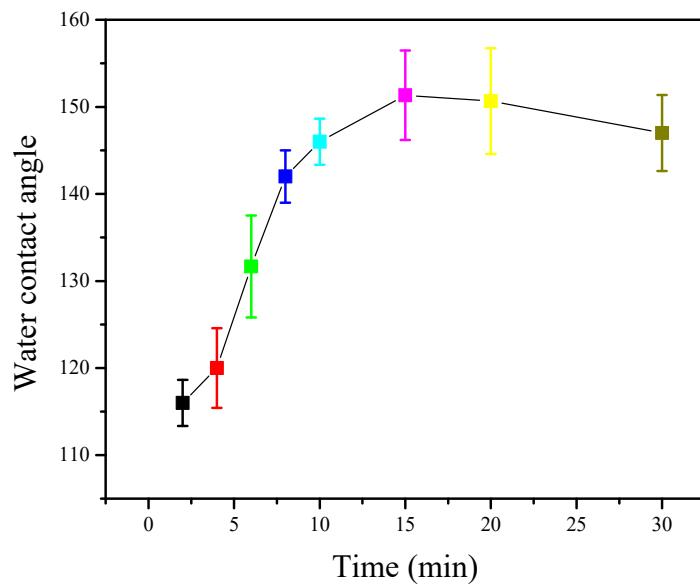


Figure S4. Water contact angle of cellulose paper changing with immersion time from 2 min to 30 min.

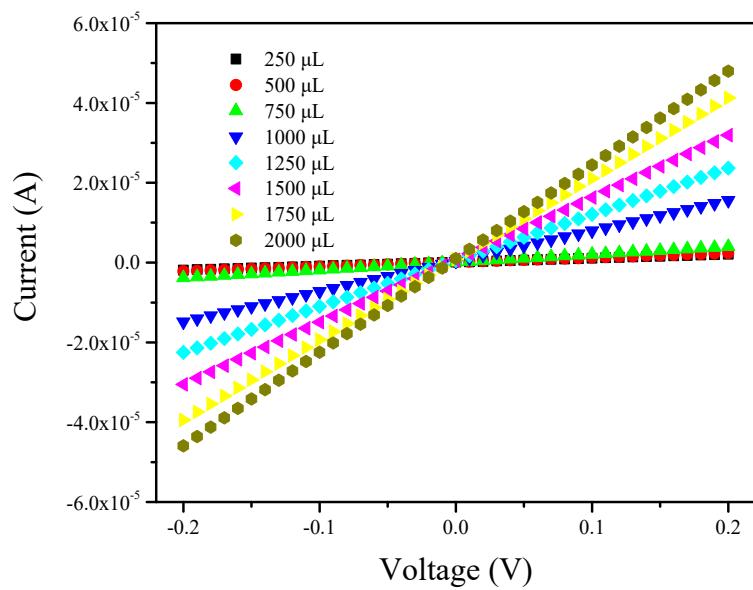
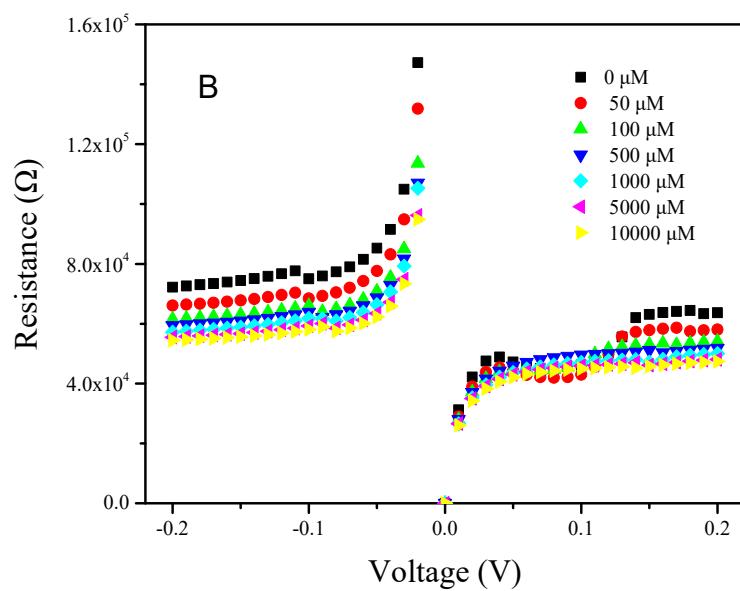
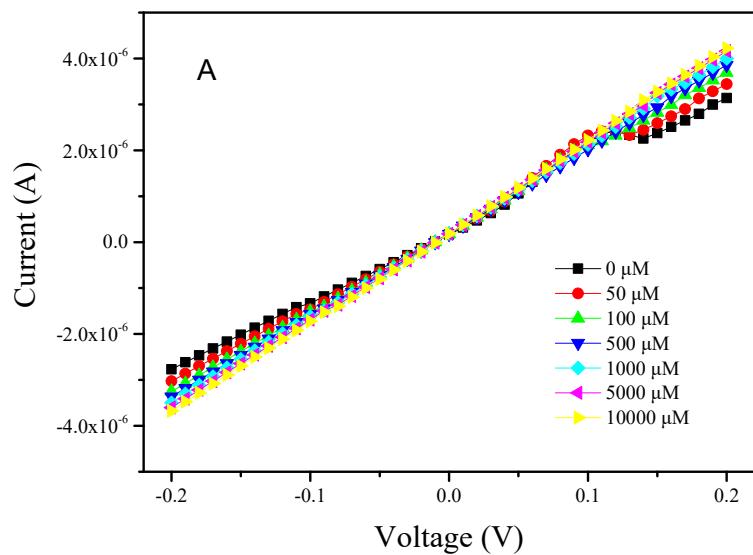


Figure S5. The I_{DS} - V_{DS} of HPFET modified with different volume of SWNTs-PCA.



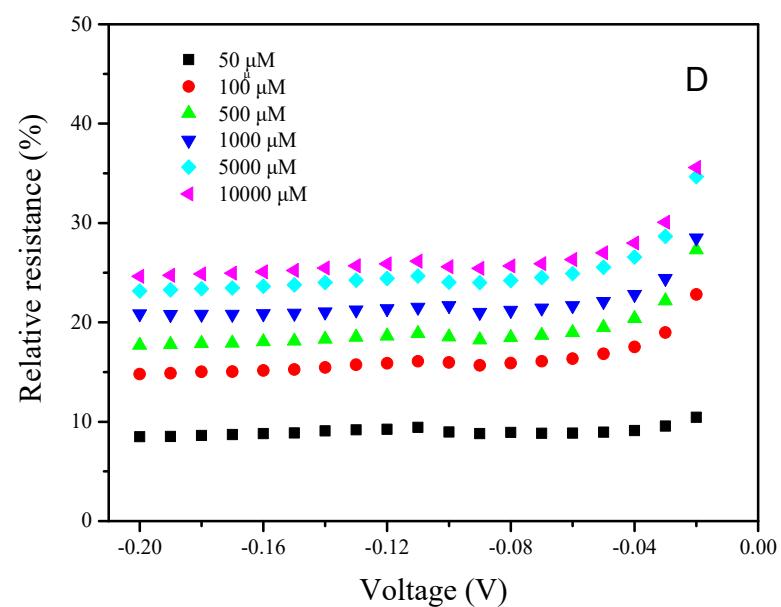
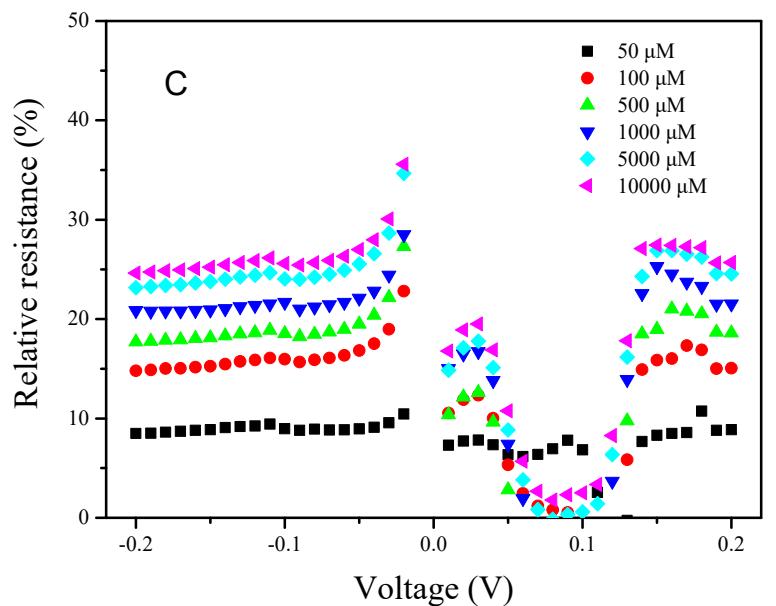


Figure S6. (A)The current-voltage of SPFET/SWNTs-PCA/DNAzyme exposure to different Ca^{2+} concentrations; (B)The resistances at each voltages after SPFET/SWNTs-PCA/DNAzyme exposure to different Ca^{2+} concentrations; (C)The relative resistances

ranging from -0.2 V to 0.2 V after SPFET/SWNTs-PCA/DNAzyme exposure to different Ca^{2+} concentrations. (D) Relative resistances of SPFET/sSWNT-PCA/DNAzyme ranging from -0.2 V to 0 V.

The cleavage efficiency of DNAzyme is associated with Ca^{2+} concentration and incubation time. Three different Ca^{2+} concentrations (100, 1000, and 10000 μM) were measured by SPFET/SWNTs-PCA/DNAzyme with varying incubation times in the range from 0 to 11 min. As shown in Figure S10, the relative resistance of SPFET/SWNTs-PCA/DNAzyme was proportional to Ca^{2+} concentrations and incubation time. For the same Ca^{2+} concentration, the relative resistance increased with incubation time, but the growth rate decreased significantly when the incubation time was higher than 7 min. For this reason, 7 min was chosen as the optimal incubation time for the experiment.

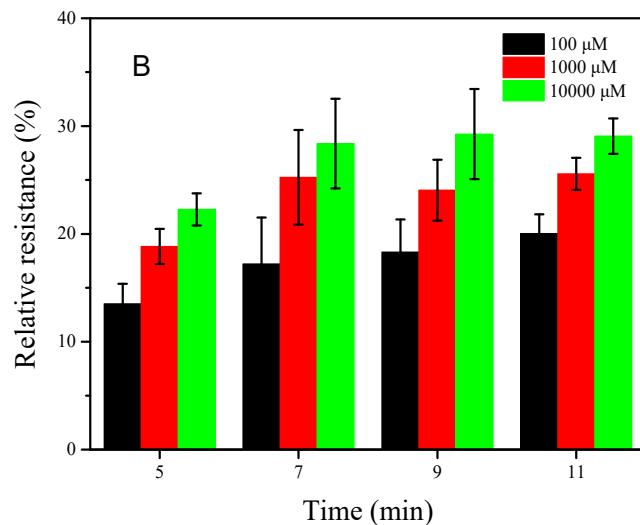


Figure S7. Relative resistances of SPFET/SWNTs-PCA/DNAzyme changing with the

incubation time in the range from 0 to 11 min for three different Ca^{2+} concentrations.

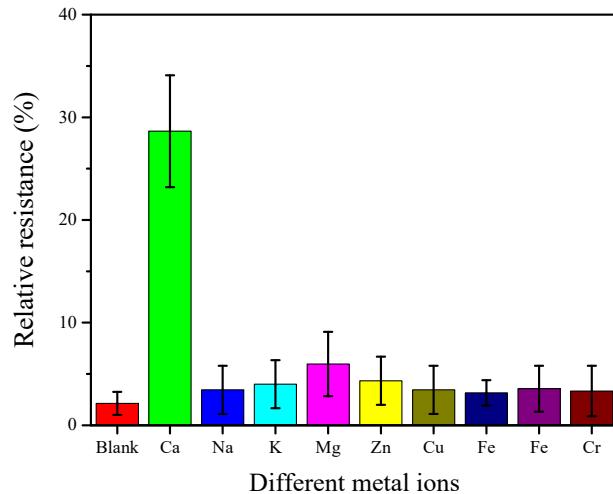


Figure S8. Relative resistances of SPFET/SWNT/DNAzyme before and after incubation in 10 mM solutions of different metal ions including Na^+ , K^+ , Mg^{2+} , Zn^{2+} , Cu^{2+} , Fe^{2+} , Fe^{3+} , and Cr^{3+} .

For SPFET/SWNTs-PCA/DNAzyme, the regression equations were $y_1 = 22.132x + 39.265$ and $y_2 = 5.4265x + 23.577$ with the R-squared of 0.9939 and 0.9782, respectively, which the detection limit was 10.7 μM (N/S=3). For SPFET/SWNTs-PCA/Nonzyme, the relative resistance revealed excellent relationship with the logarithm of Ca^{2+} concentration in the range of 0.025 mM to 10 mM. The linear regression equation was $y = 2.3384x + 4.5091$ with the linear regression correlation coefficient of 0.987.

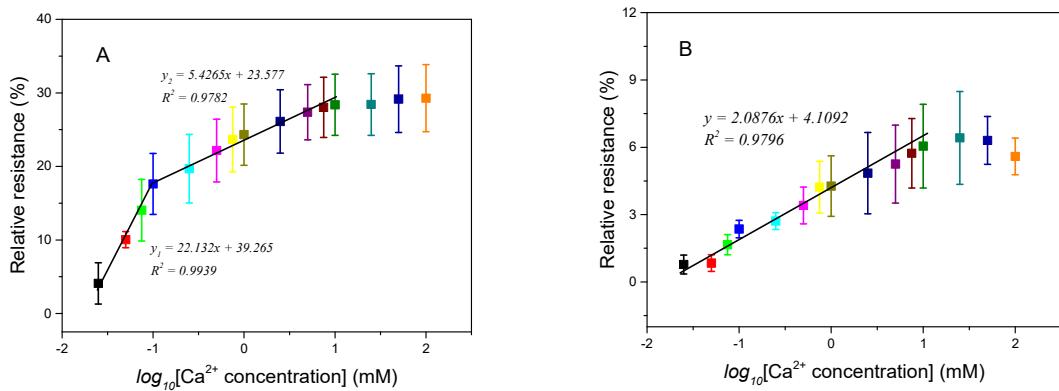


Figure S9. The linear relationship between the relative resistances of SPFET/SWNTs-PCA/DNAzyme(A) and SPFET/SWNTs-PCA/Nonzyme(B) and the logarithm of the Ca^{2+} concentration.

Table S2. Comparison of the performances of Dual-BioFET and other reported sensors for Ca^{2+} determination.

Sensor	Method	pH	Time (min)	Linear range (μM)	LOD (μM)	Ref.
Ca-ISE	Potential	2.0	1.67	$3.1 \times 10^{-3} \sim 3.2 \times 10^4$	-	¹
Ca^{2+} -SCISE	Potential	-	1.0	$1.0 \times 10^{-1} \sim 1.0 \times 10^4$	5.00	²
ECL-based ion-selective nano-optodes	Potential	7.4	-	$1.0 \times 10^0 \sim 5.0 \times 10^2$	0.11	³
Fe_2O_3 -ZnO NRs/FET	Current	7.6	-	$1.0 \times 10^1 \sim 3.0 \times 10^3$	0.05	⁴
Co_3O_4 CNT	Current	-	0.84	$1.0 \times 10^2 \sim 1.1 \times 10^4$	3.80	⁵
IS-OECT	Current	-	20	$1.0 \times 10^1 \sim 1.0 \times 10^4$		⁶
CD-EGTA	Fluorescent	7	240	$1.5 \times 10^1 \sim 3.0 \times 10^2$	0.38	⁷
DLLME	UV-visible	12.8	30	$1.5 \times 10^0 \sim 3.7 \times 10^1$	0.43	⁸
SD-ISO	Fluorescence	6.0-8.0	5	$1.0 \times 10^1 \sim 1.0 \times 10^6$	9.30	⁹
SA-4CO ₂ Et	Fluorescence	4.0-10.0	240	$6.0 \times 10^2 \sim 3.0 \times 10^3$	-	¹⁰
DNAzyme/SWNT/FET	Current	6.9	9	$1.0 \times 10^1 \sim 1.0 \times 10^3$	7.20	¹¹
Dual BioFET	Current	7.4	7	$2.5 \times 10^1 \sim 5.0 \times 10^3$	10.70	This work

CD-EGTA: carbon dot-ethylenebis(oxyethylenenitrilo)tetraacetic acid; ISO: ion-selective optode; SD: solvatochromic

dye; ISE: potentiometry based on a calcium-selective electrode; SCISE: solid-contact calcium-selective electrode; IS-OECT: ion-selective organic electrochemical transistor; SA: salicyladazine; ECL: electrochemiluminescence;

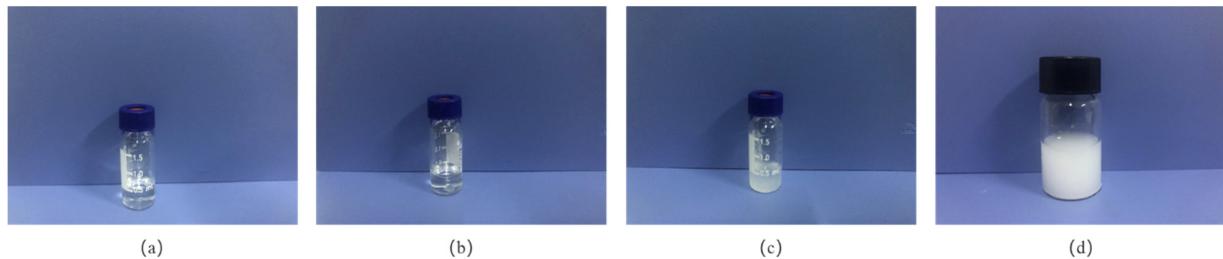


Figure S10. Preparation of superhydrophobic solution: (a) pure OTS; (b) OTS added with water; (c) mixing by vortex and sonication; and (d) incubation for 2 h under ambient conditions and dilution with hexane.

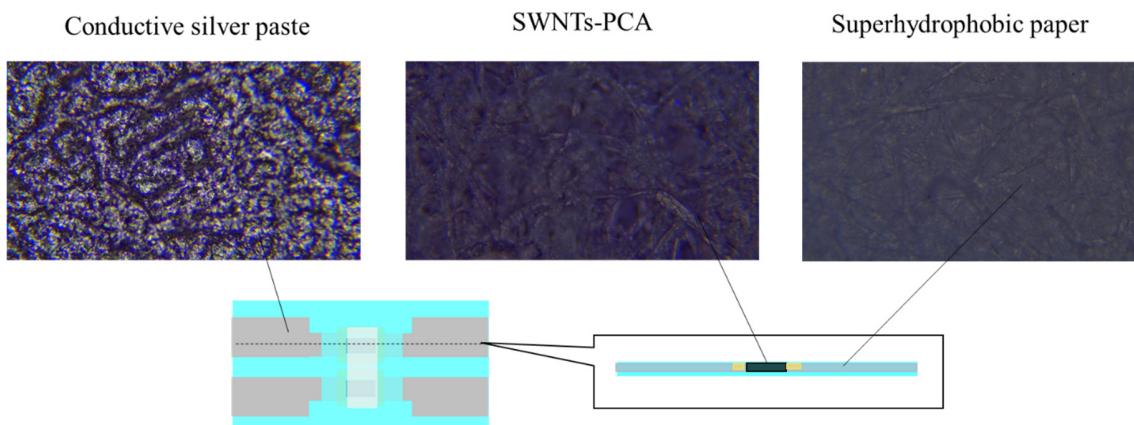
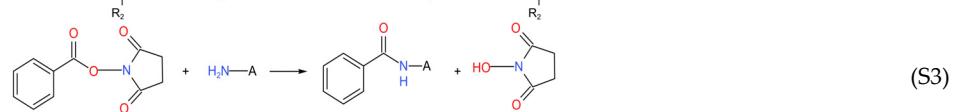
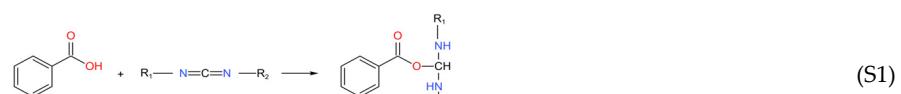


Figure S11. Structural diagram and microscope photographs of SPFET/SWNTs-PCA.



References

1. Liu, S.; Ding, J.; Qin, W. Current pulse based ion-selective electrodes for chronopotentiometric determination of calcium in seawater. *Anal. Chim. Acta* **2018**, *1031*, 67–74, <https://doi.org/10.1016/j.aca.2018.06.018>.
2. Ocaña, C.; Abramova, N.; Bratov, A.; Lindfors, T.; Bobacka, J.J.T. Calcium-selective electrodes based on photo-cured polyurethane-acrylate membranes covalently attached to methacrylate functionalized poly (3, 4-ethylenedioxythiophene) as solid-contact. *Talanta* **2018**, *186*, 279–285.
3. Zhang, J.; Chen, Y.; Fang, D. Electrochemiluminescence in Luminol-based calcium-selective nanoparticles for the determination of calcium ions. *J. Electroanal. Chem.* **2020**, *878*, 114671, <https://doi.org/10.1016/j.jelechem.2020.114671>.
4. Ahmad, R.; Tripathy, N.; Ahn, M.-S.; Yoo, J.-Y.; Hahn, Y.-B. Preparation of a Highly Conductive Seed Layer for Calcium Sensor Fabrication with Enhanced Sensing Performance. *ACS Sens.* **2018**, *3*, 772–778, <https://doi.org/10.1021/acssensors.7b00900>.
5. Yuan, H.; Ma, C.; Geng, J.; Zhang, L.; Cui, H.; Liu, C. Preparation of Co₃O₄ conical nanotube and its application in calcium ion biosensor. *Appl. Phys. A* **2018**, *124*, 101, <https://doi.org/10.1007/s00339-017-1460-x>.
6. Keene, S.; Fogarty, D.; Cooke, R.; Casadevall, C.D.; Salleo, A.; Parlak, O. Wearable Organic Electrochemical Transistor Patch for Multiplexed Sensing of Calcium and Ammonium Ions from Human Perspiration. *Adv. Heal. Mater.* **2019**, *8*, e1901321, <https://doi.org/10.1002/adhm.201901321>.
7. Yue, J.; Li, L.; Cao, L.; Zan, M.; Yang, D.; Wang, Z.; Chang, Z.; Mei, Q.; Miao, P.; Dong, W.-F. Two-Step Hydrothermal Preparation of Carbon Dots for Calcium Ion Detection. *ACS Appl. Mater. Interfaces* **2019**, *11*, 44566–44572, <https://doi.org/10.1021/acsami.9b13737>.
8. Peng, B.; Zhou, J.; Xu, J.; Fan, M.; Ma, Y.; Zhou, M.; Li, T.; Zhao, S. A smartphone-based colorimetry after dispersive liquid–liquid microextraction for rapid quantification of calcium in water and food samples. *Microchem. J.* **2019**, *149*, <https://doi.org/10.1016/j.microc.2019.104072>.
9. Shibata, H.; Ikeda, Y.; Hiruta, Y.; Citterio, D. Inkjet-printed pH-independent paper-based calcium sensor with fluorescence signal readout relying on a solvatochromic dye. *Anal. Bioanal. Chem.* **2020**, *412*, 3489–3497.
10. Gao, M.; Li, Y.; Chen, X.; Li, S.; Ren, L.; Tang, B.Z. Aggregation-Induced Emission Probe for Light-Up and in Situ Detection of Calcium Ions at High Concentration. *ACS Appl. Mater. Interfaces* **2018**, *10*, 14410–14417, <https://doi.org/10.1021/acsami.8b00952>.
11. Wang, H.; Luo, Q.; Zhao, Y.; Nan, X.; Zhang, F.; Wang, Y.; Wang, Y.; Hua, D.; Zheng, S.; Jiang, L.; et al. Electrochemical device based on nonspecific DNAzyme for the high-accuracy determination of Ca²⁺ with Pb²⁺ interference. *Bioelectrochemistry* **2020**, *140*, 107732, <https://doi.org/10.1016/j.bioelechem.2020.107732>.