

Article

Development of an Electrochemical Biosensor for the Detection of Aflatoxin M₁ in Milk

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Received: 9 September 2010; in revised form: 30 September 2010 / Accepted: 10 October 2010 /

Published: 20 October 2010

Abstract: We have developed an electrochemical immunosensor for the detection of ultratrace amounts of aflatoxin M₁ (AFM₁) in food products. The sensor was based on a competitive immunoassay using horseradish peroxidase (HRP) as a tag. Magnetic nanoparticles coated with antibody (anti-AFM₁) were used to separate the bound and unbound fractions. The samples containing AFM₁ were incubated with a fixed amount of antibody and tracer [AFM₁ linked to HRP (conjugate)] until the system reached equilibrium. Competition occurs between the antigen (AFM₁) and the conjugate for the antibody. Then, the mixture was deposited on the surface of screen-printed carbon electrodes, and the mediator [5-methylphenazinium methyl sulphate (MPMS)] was added. The enzymatic response was measured amperometrically. A standard range (0, 0.005, 0.01, 0.025, 0.05, 0.1, 0.25, 0.3, 0.4 and 0.5 ppb) of AFM₁-contaminated milk from the ELISA kit was used to obtain a standard curve for AFM₁. To test the detection sensitivity of our sensor, samples of commercial milk were supplemented at 0.01, 0.025, 0.05 or 0.1 ppb with AFM₁. Our immunosensor has a low detection limit (0.01 ppb), which is under the recommended level of AFM₁ [0.05 µg L⁻¹ (ppb)], and has good reproducibility.

Keywords: electrochemical immunosensor; aflatoxin M₁; mycotoxin; milk; horseradish peroxidase (HRP); superparamagnetic nanoparticles

with clean-up treatment by immunoaffinity columns (IC) is the reference method used for the determination of aflatoxin concentrations in milk [17]. This procedure, which is long and laborious, requires expensive equipment and well-trained personnel. Other methods for AFM₁ concentration determination have also been proposed: thin layer chromatography [18], fluorescence detection after immunoaffinity clean-up [19], liquid chromatography coupled to mass spectrometry [20] and immunoenzymatic assays.

To minimise the occurrence of AFM₁, it is essential to identify the sources of contamination using rapid, selective and sensitive assays. Immunochemical assays, which are rapid, simple, specific, sensitive and even portable, have become the most common quick methods for the routine analysis of mycotoxins in food and feed materials [21,22]. There is a need for more suitable methods, and rapid methods based on the use of biosensors or immunosensors have been proposed in the last decade [23,24]. The aim of our work was to develop a method for aflatoxin M₁ (AFM₁) detection and quantification in milk samples using an electrochemical immunosensor. A screen-printed carbon electrode is chosen as the transducer.

2. Materials and Methods

2.1. Safety notes

Aflatoxins are highly carcinogenic and should be handled with extreme care. Aflatoxin-contaminated labware should be decontaminated with an aqueous solution of sodium hypochlorite (5%). Aflatoxins are subject to light degradation; therefore, analytical work must be protected from daylight, and aflatoxin standard solutions are stored in amber vials. The use of non-acid-washed glassware for aqueous aflatoxin solutions may result in the loss of aflatoxin, and thus special attention should be paid to new glassware. Prior to use, glassware should be soaked in dilute acid (10% sulphuric acid) for several hours and then rinsed extensively with distilled water to remove all traces of acid [25].

2.2. Materials and apparatus

The I'Screen AFLA M₁ milk test kit was from Tecna s.r.l. (Trieste, Italy). Milk samples were obtained from local supermarkets. Aflatoxin M₁ from *Aspergillus flavus*, 5-methylphenazinium methyl sulphate (MPMS) and hydrogen peroxide (H₂O₂) were purchased from Sigma-Aldrich (Germany). Aflatoxin M₁ linked to horseradish peroxidase (AFM₁-HRP conjugate) from the I'Screen AFM₁ milk test kit (Tecna s.r.l, Trieste, Italy) was used. An anti-AFM₁ antibody (1 mg/mL) was purchased from Soft Flow Biotechnology (Hungary). Superparamagnetic nanoparticles (d = 300 nm), Bio-Adembeads Protein G (uniform-sized superparamagnetic nanoparticles conjugated with protein G), were from Ademtech SA (Pessac, France). Adem-Mag SV (single magnet position adapted for both 1.5/2 mL microfuge tubes or glass vials) were from Ademtech S.A. (Pessac, France). All solutions were stored in glass to limit adsorption. A horizontal shaker (IKA, vibrax, VXR) was also used for the coating step.

Chronoamperometric and cyclic voltammetric measurements were performed with an AUTOLAB PGSTAT12 potentiostat interfaced to a PC, and GPES (General Purpose Electrochemical System) software was used to collect and analyse the data (Utrecht, The Netherlands). DropSens 110 screen-printed carbon electrodes (DropSens, S.L., Spain) were used. We used a three-electrode system, with carbon working and counter electrodes and a silver reference electrode.

2.3. Reagents

Phosphate-buffered saline-Tween (PBS-T), 0.05 M, pH 7.4 (Tween-20, 0.05% v/v), and acetate buffer, 0.05 M, pH 5.2, were used.

2.4. Preparation of the AFM₁ standard range and controls

The standard range (0, 0.005, 0.01, 0.025, 0.05, 0.1, and 0.25 ppb) of the AFM₁ ELISA kit was used. To construct this standard range for AFM₁, aliquots of the 0 ppb standard milk (blank) from the ELISA kit were spiked with the stock AFM₁ solution to obtain final concentrations of 0.3, 0.4 or 0.5 ppb. The controls were prepared in PBS-T or in the 0 ppb blank from the ELISA kit. These controls were spiked with the stock AFM₁ solution to obtain final concentrations of 0.01, 0.025, 0.05 or 0.1 ppb.

2.5. Preparation of milk samples

The sample was defatted by centrifugation for 15 min at 6,000 rpm. After centrifugation, the two phases were separated, the fatty cream was discarded, and the skimmed milk was recovered and used to carry out the experimental work. Aliquots of defatted AFM₁-free milk samples were spiked with the stock solution of AFM₁ to obtain final concentrations of 0.01, 0.025, 0.05 or 0.1 ppb.

2.6. Methods and instrumentation

All affinity reactions were performed off-line by mixing the sample with the tracer (AFM₁-HRP) and antibody until equilibrium was reached.

2.7. Bead preparation

All steps (coating, competition and washing) were carried out with phosphate-buffered saline-Tween (PBS-T), 0.05 M, pH 7.4 (Tween 20 0.05% v/v). Prior to use, the suspended superparamagnetic nanoparticles conjugated with protein G were washed three times with working buffer (26 μ L beads + 1374 μ L PBS-T) to remove the ProClin 300 which acted as a preservative. The optimised procedure was as follows:

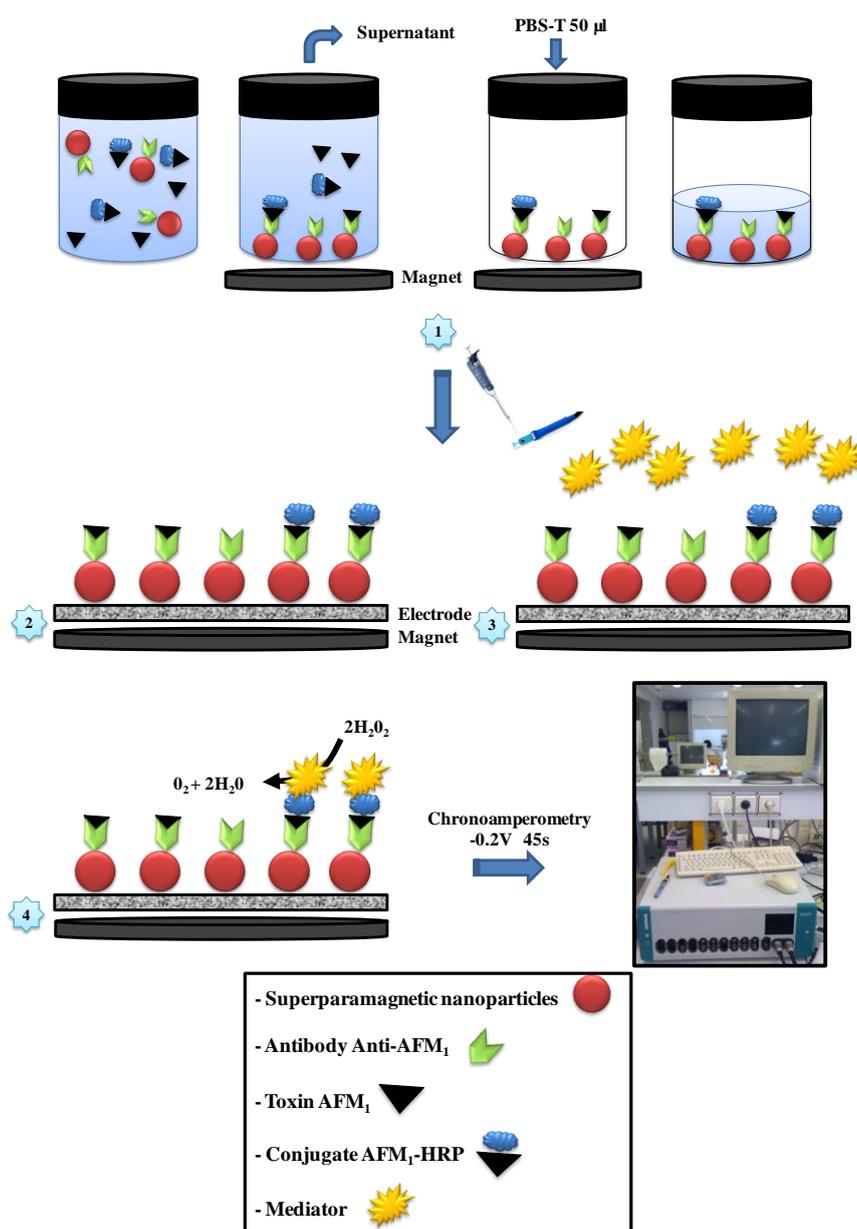
- **Coating:** the washed beads were collected using the Adem-Mag SV and the antibody solution (2 μ g/ml) prepared in working buffer (2.8 μ L antibody at 1 mg/mL + 1371 μ L PBS-T) was added and

allowed to react for 20 minutes. Then, the particles were collected using the Adem-Mag SV, washed three times with working buffer (1,400 µL) and resuspended in 1,400 µL of working buffer.

- A 101-µL aliquot of this dispersion was introduced into a glass vial, and the buffer was removed. Meanwhile, the nanoparticles were collected using the Adem-Mag SV.

- **Competition:** AFM₁ (91 µL; from the liquid standard range from the ELISA kit or spiked with milk), AFM₁-HRP solution (91 µL) prepared in working buffer (1:750 v/v) and acetate buffer (252 µL, 100 mM) were allowed to compete for antibody binding sites for 15-20 minutes. During the coating and competition steps, a horizontal shaker (200 rpm) was employed.

Figure 1. Immunosensor protocol and principle of the electrochemical immunosensor for AFM₁ detection.



2.8. Immunosensor protocol

The construction of the immunosensor required the immobilisation of the antibodies on the electrodes via the superparamagnetic nanoparticles. To this end, the screen-printed carbon electrode was placed in a magnet support to collect the superparamagnetic nanoparticles at the electrode surface (Figure 1). Then, after the competition step the particles were collected using the Adem-Mag SV, the supernatant was discarded and 50 μL of PBS-T was added to resuspend the particles (Figure 1, illustration 1), which were then introduced via a Pipetman (Gilson, France) to the surface of the screen-printed carbon electrode. Only the superparamagnetic nanoparticles remain attached to the screen-printed carbon electrode (Figure 1, illustrations 1 and 2).

Next, the electrode surface was washed with 100 μL of the mediator solution (1 mM MPMS; 10 mM H_2O_2 ; 100 mM acetate buffer) to remove all of the toxin or the conjugate that were not attached to the antibody. Before taking the measurements, 100 μL of the mediator solution was introduced to the surface of the electrode (Figure 1, illustrations 3 and 4). The measurements were carried out using a chronoamperometry method at a potential of $-0.2\text{ V vs. Ag/AgCl}$ for 45 s. All of the experiments were carried out in triplicate in independent assays.

3. Results and Discussion

This immunoassay method is based on the use of an AFM_1 -horseradish peroxidase conjugate ($\text{AFM}_1\text{-HRP}$) as a probe. HRP catalyses the oxidation of various hydrogen-donating substrates with hydrogen peroxide to produce oxidised substrate and water. MPMS and H_2O_2 were the substrates used to determine HRP activity.

First, the electrochemical behaviour of both MPMS and MPMS_{red} were investigated to optimise the conditions for the determination of HRP activity by amperometry. A cyclic voltammetric investigation of MPMS was carried out using a carbon electrode (DropSens 110). The addition of HRP to a solution containing the two substrates (MPMS and H_2O_2) led to the consumption of MPMS and consequently to a decrease in the oxidation current and an increase in the reduction current. A working potential of $-0.2\text{ V} (-200\text{ mV})$ vs. Ag/AgCl for the measurement of HRP activity was chosen for this study [26]. At this potential, the current was near zero, and no substrate reduction occurred. These conditions were optimal for enzymatic activity determinations when a small amount of product (MPMS_{red}) was measured in the presence of a high concentration of substrate.

Before testing the response of the spiked milk samples, a control assay was performed (Table 1) to verify that the AFM_1 concentration could be detected accurately by the sensor and to determine the amount of interference from the milk matrix during the measurement. For this control, PBS-T and the 0 ppb blank from the ELISA kit were spiked with the AFM_1 solution to obtain four different sample concentrations: 0.01, 0.025, 0.05 and 0.1 ppb. Electrochemical measurements of the calibration standard solutions prepared in buffer and in milk were made using the immunosensor (Table 1). The response curve for the standard series, the spiked buffer and the spiked milk were identical. Thus, the defatted milk did not affect the measurements.

Table 1. Sensor calibration using standard solutions of AFM₁ and results obtained using control samples and spiked milk.

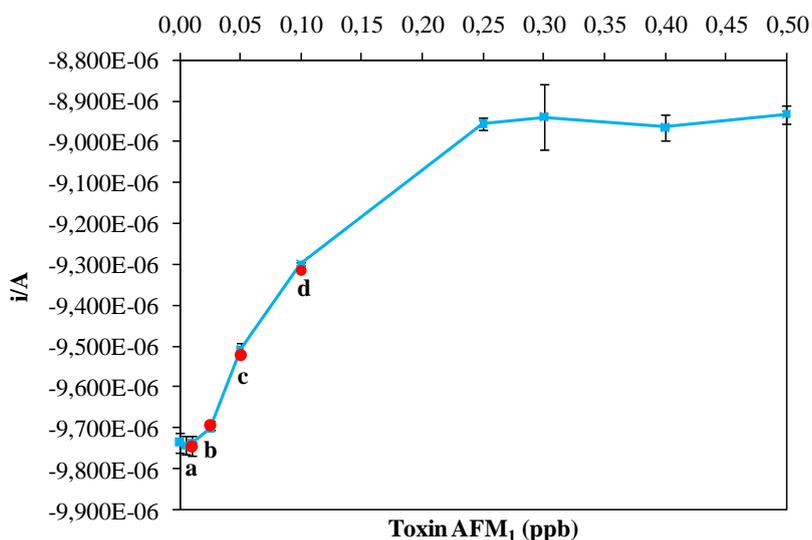
AFM ₁ standard range (ppb)	Biosensor response (A)		Control assays response (A)				Spiked milk samples response (A)		
	Mean values	Standard deviation	Spiked PBS-T	Standard deviation	Spiked 0 ppb ELISA Kit Blank	Standard deviation	Mean values	Standard deviation	References
0	-9.735E-06	2.46E-08							
0.005	-9.743E-06	2.35E-08							
0.01	-9.738E-06	4.93E-09	-9.74E-06	8.60E-08	-9.73E-06	8.35E-08	-9.745E-06	1.617E-08	a
0.025	-9.702E-06	3.06E-09	-9.70E-06	4.00E-08	-9.69E-06	3.91E-08	-9.694E-06	1.528E-09	b
0.05	-9.508E-06	1.48E-08	-9.58E-06	2.98E-08	-9.56E-06	4.68E-08	-9.523E-06	2.442E-08	c
0.1	-9.300E-06	3.61E-09	-9.30E-06	1.89E-08	-9.32E-06	6.64E-08	-9.316E-06	1.106E-08	d
0.25	-8.956E-06	1.53E-08							
0.3	-8.939E-06	7.90E-08							
0.4	-8.965E-06	3.11E-08							
0.5	-8.932E-06	2.28E-08							

References: (a) 0.01 ppb; (b) 0.025 ppb; (c) 0.05 ppb; (d) 0.1 ppb

After this first step, which validated the immunosensor protocol, we performed the second step of our experiment with real milk samples. The milk used for the standard range came from the ELISA kit, as in the first experiment, and experimental milk samples were from commercial sources.

We constructed a standard curve to determine the relationship between the concentration of AFM₁ in the sample and the measured intensity. With this standard curve (Figure 2, blue squares), we also calculated the upper and lower limits of detection of the immunosensor. The detection limits of AFM₁ by the sensor were 0.25 µg L⁻¹ (ppb) for the upper limit and 0.01 µg L⁻¹ (ppb) for the lower limit (Figure 2 and Table 1).

Figure 2. Curve of the AFM₁ standard range (blue squares) and the spiked AFM₁ milk samples a, b, c and d (red circles). Vertical bars represent standard errors (not shown when smaller than the symbols).



In the second part of the experiment, commercial milk samples contaminated with a known concentration of AFM₁ (0.01, 0.025, 0.05 or 0.1 ppb; references a, b, c, d in Table 1 and Figure 2) were tested. The intensity responses for each concentration were measured. The values for the spiked milk samples were the similar to those values measured for the standard range (Table 1 and Figure 2, red circles). The analytical performance of our approach is better for the low concentrations of toxin in comparison with the other. For example, Badea *et al.* [23] realized an flow injection immunoassay system for aflatoxin M₁ determination and with our approach we have the same limit of detection for the high concentration (0.5 ppb) but we have a higher sensitivity for the lower concentration (0.01 ppb), the same as the system developed by Carlson *et al.* [24].

Our immunosensor allows the detection and the quantification of AFM₁ over a large range of concentrations. Our immunosensor allows the estimation the real contamination level of spiked milk samples.

4. Conclusions

This immunosensor has a working range that is comparable or better than that found for conventional methods. The detection range of 0.01 to 0.1 ppb obtained for milk samples allows the use of this method in dairy industry laboratories. The use of this immunosensor can ensure that the milk purchased by consumers is harmless. Our system allows the measurement of AFM₁ directly in milk after a single centrifugation step without dilution or pretreatment steps. Another advantage of our method is that the analysis time is reduced and the sample preparation is very simple and fast in comparison with the conventional methods (HPLC and ELISA, for example).

The goal of developing a method using magnetic beads was to optimise this immunosensor by developing a protocol that will allow automation of the sanitary control of foodstuffs. Future work will investigate the development of this immunosensor using flux methods. If the optimisation of a flow-injection system immunoassay for AFM₁ could be realised, then this assay system would be a good method for the rapid screening of raw milk samples for this toxin. This immunosensor is inexpensive, easy to operate and very suitable to automation.

Acknowledgements

The authors are grateful to EraSME (*Food for better human health program*) for financial support for the project Real Time Aflatoxin M₁ Biosensor Development.

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